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SUPPLEMENT

The Massachusetts General Hospital acute stroke imaging algorithm: an experience and evidence based approach

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ABSTRACT

The Massachusetts General Hospital Neuroradiology Division employed an experience and evidence based approach to develop a neuroimaging algorithm to best select patients with severe ischemic strokes caused by anterior circulation occlusions (ACOs) for intravenous tissue plasminogen activator and endovascular treatment. Methods found to be of value included the National Institutes of Health Stroke Scale (NIHSS), non-contrast CT, CT angiography (CTA) and diffusion MRI. Perfusion imaging by CT and MRI were found to be unnecessary for safe and effective triage of patients with severe ACOs. An algorithm was adopted that includes: non-contrast CT to identify hemorrhage and large hypodensity followed by CTA to identify the ACO; diffusion MRI to estimate the core infarct; and NIHSS in conjunction with diffusion data to estimate the clinical penumbra.

INTRODUCTION

The purpose was to use an experience and evidence based approach to develop the neuroimaging algorithm that best improves outcomes in patients with severe ischemic strokes caused by anterior circulation occlusions (ACOs). Patients with these strokes account for the majority of individual, family, and societal costs due to stroke, and they are treatable with intravenous (IV) tissue plasminogen activator (tPA) or/and intra-arterial therapy (IAT). Critically evaluated was the capability of each specific method to provide reliable information on three key components of stroke physiology: (1) site of arterial occlusion; (2) extent of irreversibly injured tissue ('infarct core'); and (3) the size of the ischemic penumbra (figure 1). Although varying definitions of the ischemic penumbra exist, the penumbra is defined herein as severely hypoperfused brain tissue that may eventually be recruited into the infarct core, if not reperfused quickly enough.¹

METHODOLOGY

The critical physiological information in the acute stroke patient with severe symptoms is shown in figure 1, which is a representation of a patient with a proximal right middle cerebral artery occlusion. Individual neuroradiology and neurology faculty from the Massachusetts General Hospital (MGH) presented the best evidence from the literature and

clinical experience on the value of each method. Expert opinions were presented for the National Institutes of Health Stroke Scale (NIHSS), non-contrast CT (NCCT), CT angiography (CTA), CTA source images (CTA-SI), diffusion MRI, CT perfusion (CTP), and MRI perfusion (MRP). Faculty and fellows who did not present but heard the evidence, met to weigh the evidence and make recommendations. Each modality was assessed on two different sets of criteria shown in tables 1 and 2. The basic practical question was: 'Is the modality valuable for patient care and can we obtain it in an acute setting?' In addition to traditional metrics such as sensitivity and specificity, the following factors were factored into the assessments:

- **Workflow.** Place of the imaging test in the workflow and does it negatively or positively affect the workflow when an acute stroke patient arrives in the emergency department.
- **Repeatability.** The values measured by the imaging test are not affected by extraneous parameters and repeated invocations of the test would result in the same conclusions.
- **Reliability.** Measured values reflect the purported physiologic parameter about the patient condition.
- **Clinical efficacy.** The imaging test improves patient outcomes.

ISCHEMIC STROKE THERAPY

Intravenous tissue plasminogen activator

Intravenously administered tPA is a proven effective treatment for ischemic stroke.² The primary indicators for its administration are an elapsed time since onset of 4.5 h or less and an absence of hemorrhage or large infarct on imaging, usually NCCT.

Intra-arterial therapy

The target of IAT is a proximal artery occlusion. The focus here is on major ACOs which account for approximately 90% of all such occlusions.³ In patients with blockages of the intracranial internal carotid artery (ICA) or middle cerebral artery stem (M1 segment), two recent studies have demonstrated the critical role of infarct volume in determining long term functional outcome (figure 2).^{4,5} When patients have large final infarcts, there is a high likelihood of significant disability or death. It

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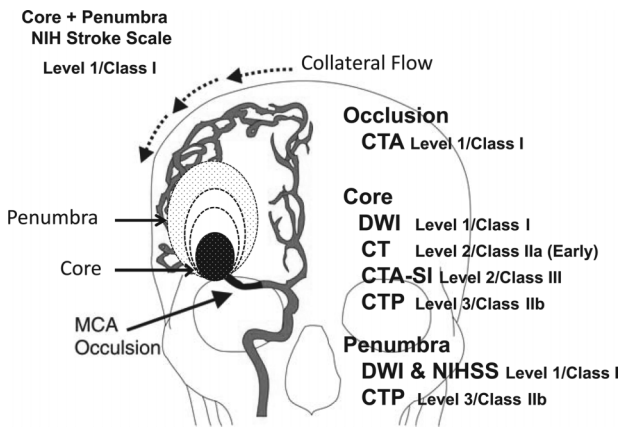


Figure 1 Measurements of physiological components of middle cerebral artery (MCA) occlusion. Depicted is a representation of a right MCA occlusion with a growing infarct core coupled to a shrinking penumbra at a rate determined by collateral flow. The value of each method used to measure each component of stroke physiology is shown, as judged according to criteria stated in the methodology and in tables 1 and 2. CTA, CT angiography; CTA-SI, CT angiography-source images; CTP, CT perfusion; DWI, diffusion weighted imaging; NIHSS, National Institutes of Health Stroke Scale.

follows then that patients presenting with extensive infarction (ie, >70–100 ml) before treatment will have little chance for a good IAT response.^{6,7} Moreover, studies have shown that the risk of reperfusion hemorrhage increases with pretreatment infarct size, and is very high (~15%) when infarcts are larger than 100 ml.^{8,9} Therefore, risk outweighs benefit in this subset of patients. Numerous studies have confirmed the importance of core infarct size in predicting IAT outcomes.^{6,7,10–12} The decision to proceed to IAT therefore critically depends on the size of the infarct core at the time of treatment, and the primary role of imaging after identification of a treatable occlusion is to reliably define core infarct size accurately and precisely.

ASSESSMENT OF METHODS

National Institutes of Health Stroke Scale

The NIHSS is a Level 1/Class I test in the assessment of the acute stroke patient.² It helps to quickly determine if the patient is having a stroke and gives an indication of the severity of the

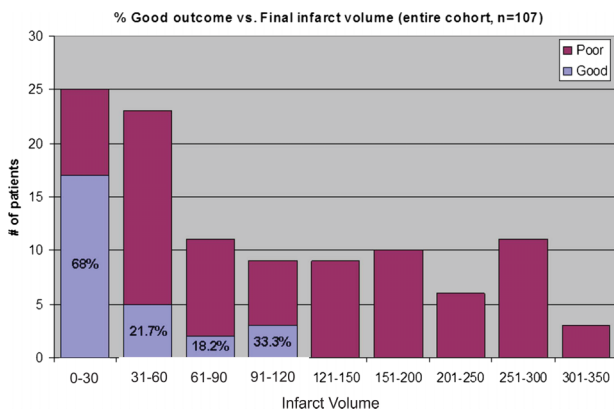


Figure 2 Relationship of final infarct size to clinical outcomes in patients with major anterior circulation occlusions (ACO) treated endovascularly. The bar graphs depict the proportion of good outcomes defined as a modified Rankin Scale score of 0–2 at 3 months (blue bars) by final infarct volume strata. The data are from 107 patients with ACO. The figure was derived from Yoo *et al.*⁴

Table 1 Massachusetts General Hospital experience and practice based criteria

Level 1	Nearly always valuable in patient care, and successfully obtainable in the vast majority of patients
Level 2	May be valuable in patient care, and is successfully obtainable in most patients
Level 3	Valuable for research purposes and may or may not help in the management of the patient

stroke. It provides a clinically relevant estimate of the size of the ischemic tissue at risk but cannot differentiate the core from the penumbra.

Non-contrast CT

NCCT is a Level 1/Class I test for excluding intracranial hemorrhage and mass lesions.² Because of the low sensitivity, NCCT was scored Level 2/Class IIa to detect the infarct core volume during the first few hours after stroke onset. The place of NCCT in the workflow and the order of imaging modalities were also considered and it was agreed that NCCT should be the first test in the evaluation of acute stroke. There are exceptions—for example, MRI could be undertaken as the first imaging study in patients with poor renal function who cannot get CTA, young patients presenting with acute stroke, or patients more likely to have a non-ischemic etiology, such as a mass, seizure, or migraines as the cause of their presenting symptoms.

CT angiography

CTA is a Level 1/Class I test for the rapid assessment of large vessel occlusion.^{2,13–15} It may also be effective for detection of medium and small vessel occlusions, even though they can take longer to find. There was no concern regarding repeatability, reliability, clinical efficacy, or overall utility of CTA. It was agreed that CTA should be performed immediately after the NCCT scan, when feasible.

CT angiography source images

CTA-SI have been suggested as a surrogate for the infarct core. Some older studies suggested that CTA-SI can image ischemic core.^{16,17} However, tissue density in CTA-SI is heavily dependent on the scan timing, cardiac output, the rate of injection, and the osmolality of the contrast media, among other parameters. For these reasons, questions were raised about the repeatability and reliability of CTA-SI in measuring tissue perfusion. Overall,

Table 2 Evidence based classification of recommendations

Class I	An imaging modality for which there is evidence for and/or general agreement that it is beneficial, useful, and effective in the management of acute stroke
Class II	An imaging modality for which there is conflicting evidence and/or divergence of opinion about the usefulness/efficacy in the management of acute stroke
Class IIa	Weight of evidence or opinion is in favor of the usefulness or efficacy of this imaging modality
Class IIb	The usefulness or efficacy is less well established by the evidence or expert opinion
Class III	An imaging test for which there is evidence and/or general agreement that it is not useful or effective, and in some cases may be harmful, in the management of acute stroke patients

CTA-SI was judged to be a Level 2/Class III examination in eliciting the core of an ischemic infarct.

Diffusion MRI

Diffusion MRI is a Level 1/Class I test for the early detection of infarct core. Diffusion weighted imaging (DWI) is nearly 100% sensitive and specific in diagnosing acute stroke^{18–25} although it is not perfect in identifying the infarct core. Positron emission tomography (PET) studies have shown that some non-viable tissue occasionally may not demonstrate restricted diffusion^{26–27}. Also, DWI abnormalities are sometimes reversible.^{28–33} However, reversal of a DWI abnormality is unusual.^{34–7} When DWI reversal does occur, it usually involves only a small part of the lesion.³⁵ Also, most of the time, the apparent DWI reversal is actually a pseudo-reversal, in that the tissue involved proceeds to infarction anyway.^{7, 31–33}

Perfusion imaging

Brain perfusion imaging provides information on cerebral hemodynamics imbedded in parameters such as cerebral blood flow (CBF), cerebral blood volume (CBV), and mean transit time (MTT). Perfusion imaging may provide many types of important information in the care of acute stroke patients.^{36–37} Additionally, much research has been devoted to demonstrating that perfusion imaging can identify the core and penumbra, and that perfusion imaging is useful for identifying patients with major ACOs that are suitable for interventional therapy.^{2, 38–39} However, evidence based reviews have questioned this.^{2, 40–41}

Perfusion imaging: theoretical considerations

Perfusion imaging studies the hemodynamic status of the brain at one instant in time, and there is no instantaneous hemodynamic state that uniquely characterizes the infarct core. The hemodynamic response of the brain to ischemia has been characterized with respect to cerebral perfusion pressure, and perfusion parameters are summarized in figure 3 (and in more detail in the online supplementary appendix figure A1). The autoregulatory vasodilation in response to reductions in regional cerebral perfusion pressure would be expected to result in increased, rather than decreased, CBV in ischemic tissue. Indeed, CBV may be elevated more often than reduced in the infarct core.⁴² More recent proposals have suggested that regions of sufficiently reduced CBF may be labeled as infarct core. This approach has greater pathophysiologic validity in that CBF reflects the rate of delivery of oxygen and glucose to brain tissue, and reductions in this rate of delivery are responsible for ischemic cell death. However, neither CBF nor any other hemodynamic measurement could ever be used to identify the core. Even complete cessation of blood flow can persist for several minutes without causing irreversible damage. Obviously, perfusion imaging demonstrates no evidence of ongoing perfusion impairment in reperfused tissue.

There are several hemodynamic measurements that are time related with no direct relationship to threats to tissue viability. For example, one of these measurements, Tmax, reflects the time that elapses between arrival of blood in an index artery and its arrival in brain tissue. A delay in the arrival of blood does not directly threaten tissue survival. MTT measures the average amount of time that blood spends in brain tissue, which is usually prolonged in underperfused brain tissue. In the setting of proximal ACO, blood must reach the tissue bed via collateral pathways whose increased circuitry would be expected to result in delayed arrival—that is, increased Tmax. Also, occlusion of a proximal artery would be expected to result in at least some

	CBV	CBF	MTT	Tmax
Alternate pathway, CPP preserved	—	—	—	↑
Compensated low CPP	↑	—	↑	↑
Underperfused	↑↓	↓	↑↓	↑
Overperfused (post-ischemic hyperperfusion)	↑	↑	↑↓	↑↓

Figure 3 Changes in hemodynamic parameters that may occur in major anterior circulation occlusions. The change in cerebral perfusion pressure (CPP) may or may not be fully compensated by the collateral circulation. In each of the four scenarios, arrows indicate possible increase or decrease in cerebral blood volume (CBV), cerebral blood flow (CBF), mean transit time (MTT) and Tmax. This is a derivation of the more detailed graph shown in the online supplementary appendix figure A1.

reduction in distal perfusion pressure, which would cause compensatory vasodilation in some of the downstream tissue. This vasodilation by itself should result in prolongation of MTT.

Thus patients with major ACO may or may not have large regions with reduced CBF but virtually all of these patients will demonstrate large regions of MTT and Tmax elevation. Empirically, we have shown this to be the case, as demonstrated in the online supplementary appendix figure A2.^{43–44} In general, the existence of a large region with increased Tmax and MTT may be inferred from the existence of a proximal artery occlusion on CT or MR angiographic imaging alone.

CT perfusion

Several issues and concerns about CTP were raised in addition to radiation exposure. These concerns—which are related to the workflow, process of obtaining CTP maps, and the utility of the information derived from a CTP study—are summarized below.

CTP process and workflow

There is a lack of clear guidelines on when CTP should be performed, and how it should be interpreted. There was broad agreement that:

- ▶ Quantification of perfusion using CTP is not validated.
- ▶ There is high inter-vendor variability.
- ▶ There is high intra-vendor variability based on the software version used.
- ▶ The variability in CTP maps is as yet unquantified with respect to the variations in heart rate, blood pressure, ejection fraction, rate of infusion, osmolality of IV contrast, rotation time, and temporal resolution of the scanner.⁴⁵
- ▶ The efficacy of CTP in improving patient outcomes is unproven.

Studies performed at MGH directly comparing core volumes by DWI and CTP in patients with severe strokes with ACOs revealed statistically significant high correlations between the two methods. However, while there is good correlation in a population, there is a wide clinically relevant discordance

between DWI and CTP derived core volumes in individual patients (see online supplementary appendix figure A3).

The above considerations led to the following guidelines on the use of CTP:

- ▶ CTP is a Level 3/Class IIb method for early estimation of the infarct core in acute stroke patients. Because CTP is unable to adequately estimate the core, it necessarily follows that it is a Level 3/Class IIb method for estimation of the penumbra.
- ▶ CTP has no proven role in selecting ACO patients for IV thrombolysis or endovascular therapy. Its roles should be limited to:
 - Research patients
 - Patients who cannot get a diffusion weighted MRI
 - Perfusion data could be used for other purposes such as hypertensive therapy. However, there are scant data on this application.

MR perfusion

MRP was deemed preferable to CTP because there is no radiation exposure and it has a generally superior workflow. However, the repeatability, reliability, and clinical efficacy of MRP raise similar concerns to those of CTP, including:

- ▶ Quantification using MR perfusion maps is not validated.
- ▶ There is high inter-vendor variability.
- ▶ The variability of MRP maps with respect to physiologic variables (eg, heart rate, blood pressure, ejection fraction) and scan parameters (eg, rate of infusion, osmolality of IV contrast, rotation time, etc) is unknown.

Carroll and colleagues⁴⁶ performed a Bland–Altman analysis of eight smokers who were imaged with MRP and H₂ ¹⁵O PET and concluded that “Until reproducibility is improved, MR is not suitable for reliable quantitative perfusion measurements”. Other research assessing the reliability of MRP was also reviewed. For example, Takasawa and colleagues⁴⁷ studied perfusion MR (deconvolution method) and PET in five patients, back to back, at a mean time interval of 16 h after stroke onset. The authors concluded that “MRP appears sufficiently reliable for clinical purposes”. However, most participants deliberating on the value of the methods thought that reliability does not override the concerns regarding high variability and low repeatability.

Overall, MRP was judged to be a Level 3/Class IIb technique in the management of acute stroke. There was broad agreement that:

- ▶ MRP has no proven role in selecting ACO patients for endovascular therapy. There is preliminary evidence that it may improve patient selection for intravenous thrombolysis but this evidence is currently insufficient to justify MRP’s clinical use in this role.
- ▶ Clinical indications for MRP may include:
 - Research patients
 - If perfusion data are deemed essential for evaluating the full clinical picture
 - When perfusion data can be used for other purposes such as hypertensive therapy, although there are few data on this.

The clinical penumbra

The evidence supports that the clinical penumbra, as measured by a combination of the NIHSS and the core determined by DWI, is the best indicator of a poor outcome in the absence of timely reperfusion. The Prolyse in Acute Cerebral Thromboembolism II trial demonstrated that patients with NIHSS scores <10 did not derive a clinical benefit from IAT.⁴⁸ This is due to the relatively good natural history in this subset

of patients.⁴⁹ Approximately one-third of the middle cerebral artery M1 segment occlusions present with such low scores.⁵⁰ The evidence best supports the following definition of a clinically significant penumbra: (1) major anterior circulation (ICA terminus or M1) occlusion; (2) NIHSS score >10; and (3) small core infarct size (DWI lesion volume <70). Both NIHSS and DWI are Level 1/Class I tests; together it is judged to be a Level 1/Class I method to assess the clinically relevant penumbra.

THE MGH STROKE IMAGING ALGORITHM

Based on the conclusions of the evaluation committee on the value of each method delineated above, a new imaging algorithm was proposed and adopted. A diagram of the algorithm is shown in figure 4. Briefly, all patients presenting with a stroke syndrome receive a neurological evaluation, including the NIHSS. NCCT is performed followed by CTA. If NCCT does not demonstrate hemorrhage or large hypodensity, and the patient is within the time window, tPA is prepared while the CTA is performed, and infusion begins once it is prepared. If the patient has a distal ICA and/or proximal middle cerebral artery occlusion, he/she is moved to the MRI scanner where diffusion MRI is performed. If the DWI lesion is small (<70 ml), the patient is sent for IAT if the additional clinical and medical criteria are met. Perfusion imaging with CT or MRI may be performed if these conditions

MGH Acute Stroke Imaging Algorithm

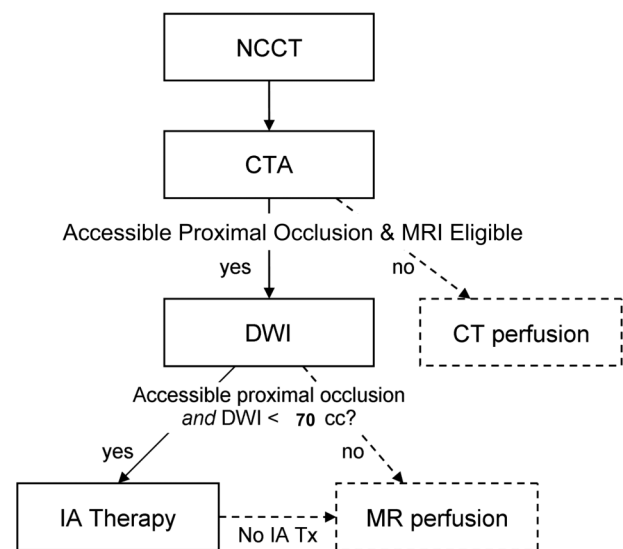


Figure 4 Massachusetts General Hospital acute stroke imaging algorithm for triage of patients with severe ischemic strokes caused by anterior circulation occlusions. All patients undergo non-contrast CT (NCCT) followed by CT angiography (CTA). If the patient has severe neurological deficits (National Institutes of Health Stroke Scale score ≥ 10), no large hypodensity and no hemorrhage on NCCT, and an occlusion is identified of the distal internal carotid artery and/or proximal middle cerebral artery that is accessible by microcatheter, then the patient is immediately evaluated by diffusion MRI if there are no contraindications to MRI. If the diffusion weighted imaging (DWI) lesion is small, defined as <70 ml, then the patient is immediately triaged to endovascular therapy if the patient is otherwise eligible for such treatment. If the patient is not eligible for MRI, he/she may undergo a CT perfusion study for possible guidance for therapy or for prognostic information. Also, if the patient is not eligible for endovascular therapy, CT or MR perfusion may be performed for similar reasons. Only the first step in this algorithm (NCCT) and the time from stroke onset are needed for the decision to treat with intravenous tissue plasminogen activator. IA, intra-arterial.

are not met, the patient cannot be scanned by MRI, or is not otherwise eligible for IAT and there is relevant clinical information that may be provided by the perfusion data.

After the algorithm was adopted, there was a significant decline in the number of perfusion CT examinations performed, as shown in the online supplementary appendix figure A4. From 40–50 CTP examinations per month in stroke patients performed during the peak years of 2005–2008, it fell to approximately 10 per month. There has been no discernible effect on patient outcomes.

Contributors All authors contributed to the manuscript and study.

Competing interests JMR is on the imaging committee of the DIAS trial for Lundbeck Pharmaceuticals. MHL has research support from GE Healthcare and is a consultant for Millenium Pharmaceuticals.

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Appendix Figures

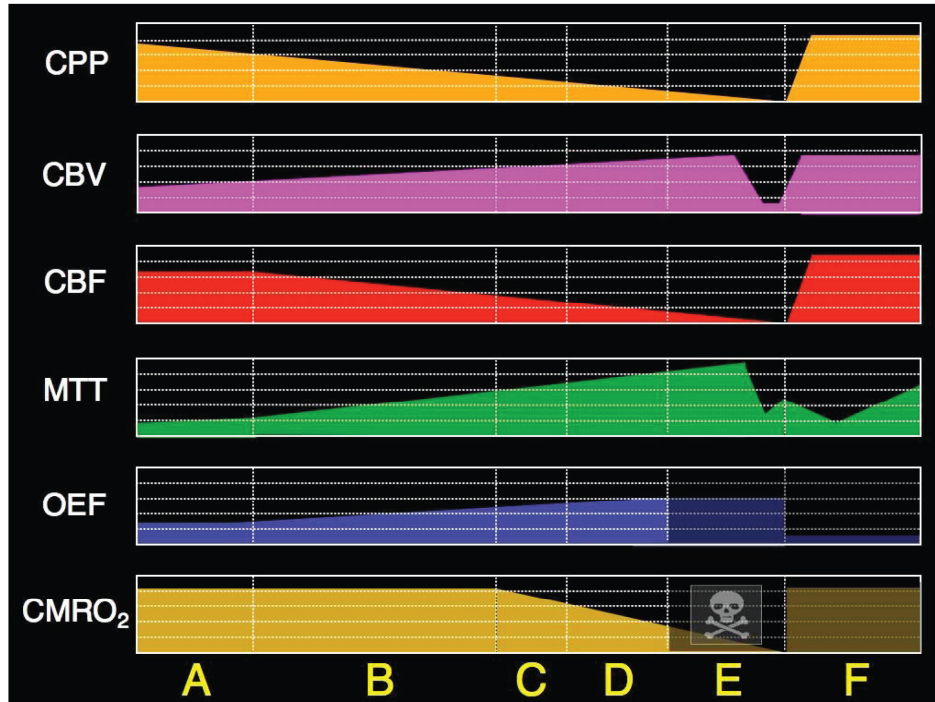


Figure A1

Figure A1. Hemodynamic changes that may occur in major anterior circulation occlusions. Cerebral perfusion is driven fundamentally by regional cerebral perfusion pressure (CPP). In response to mild decreases in CPP, precapillary resistance vessels dilate, in order to reduce cerebrovascular resistance. This is manifested by an increase in cerebral blood volume (CBV). If the reduction in vascular resistance is sufficient to maintain normal cerebral blood flow (CBF), this condition may be considered to be a compensated reduction in CPP (A). Note that

mean vascular transit time (MTT), which is the quotient of CBV divided by CBF, is increased in this condition.

With more severe reductions in CPP, autoregulatory vasodilation is insufficient to maintain normal CBF (B) CBF falls below normal levels, and therefore brain tissue experiencing this condition (and also hemodynamic conditions C through E) may be called “underperfused.” MTT continues to increase, and this has the following protective effect upon the brain. When blood spends more time in gas-permeable capillaries, brain cells are able to extract a greater proportion of the blood’s oxygen. As a result of this increase in oxygen extraction fraction (OEF), the brain’s required oxygen supply is maintained, and the cerebral metabolic rate of oxygen consumption, CMRO₂, is preserved. OEF and CMRO₂ can be measured by PET, and ongoing developments in MRI technology hold the promise of measuring these quantities in the future.

If CPP falls further, OEF is maximized, and the brain’s supply of oxygen begins to fall short of its metabolic needs (C). CMRO₂ begins to fall, and lactate accumulates as a result of anaerobic glycolysis. However, a sufficiently mild drop in CMRO₂ neither threatens tissue viability, nor results in clinically detectable electrical dysfunction. The conditions defined by (B) and (C) are sometimes called “benign oligemia.”

A further reduction in CPP results in neuronal electrical failure (D), and therefore the possibility of a clinically observable neurologic deficit. However, the CBF threshold for electrical function is below the threshold for tissue viability, and

therefore some electrically silent tissue may persist indefinitely as such, without threat to its survival.

A sufficient reduction in CBF causes infarction (E). Importantly, the time that it takes for ischemic damage to become irreversible is inversely related to the severity of the ischemia. A complete cessation of blood flow causes cell death in minutes, whereas tissue may survive a less severe reduction in CBF for hours, before being rescued by reperfusion. The irregular graphs of CBV and MTT reflect the hypothesis in (E) reflect the hypothesis that, when CPP is extremely low, the elevation of CBV that is usually seen in ischemic may be reversed, and CBV may fall below normal, either because blood vessels collapse, or because extremely slow blood flow results in intravascular thrombosis. The phenomenon of CBV reduction has been incompletely researched, and it is not clear how often it occurs.

Reperfusion of previously ischemic tissue frequently occurs spontaneously, and may also result from therapeutic intervention. Following reperfusion, autoregulatory impairment often results in persistent vasodilation following restoration of normal CPP, a condition called post-ischemic hyperperfusion (F). CBV and CBF are both elevated above normal levels. Their quotient, MTT, may be either elevated or decreased, although the latter seems more common. Figure adapted by William A. Copen, MD from Powers WJ, et al. [1 2]

Mismatch in MCA/ICA Occlusions

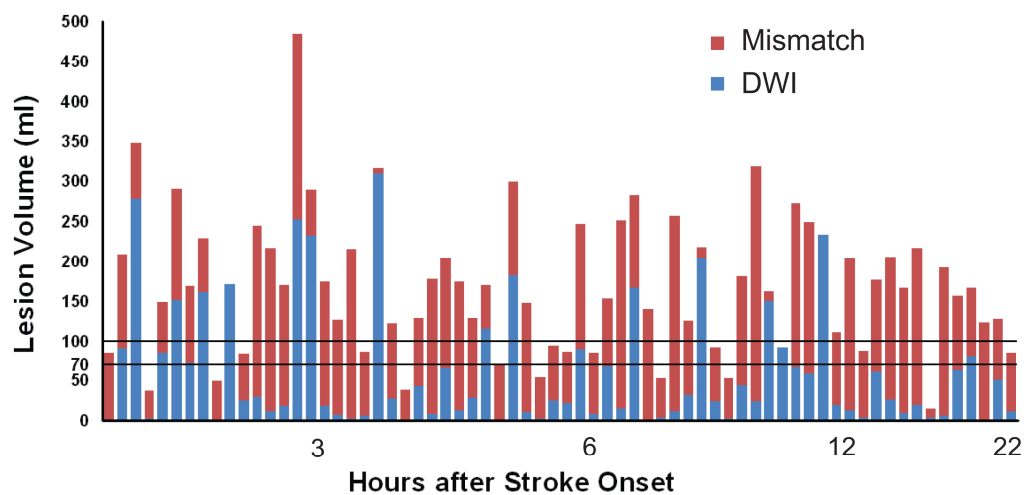


Figure A2

Figure A2. DWI/MTT mismatch volumes of 68 consecutive patients with anterior circulation occlusion in order of time after stroke onset. Abnormal DWI volume of each patient is depicted as a blue bar. Red bars represent DWI/MTT mismatch. Horizontal lines demarcate volumes of 70 ml and 100 ml. Time since stroke onset is in hours. All patients with DWI lesion volume 70 ml or less had at least a 100% mismatch. There was no significant correlation between time from stroke onset and DWI lesion volume or between time and mismatch volume. DWI: Diffusion weighted imaging; MTT: Mean transit time. [3 4]

Correlation between DWI and CTP-CBF in Same Patients

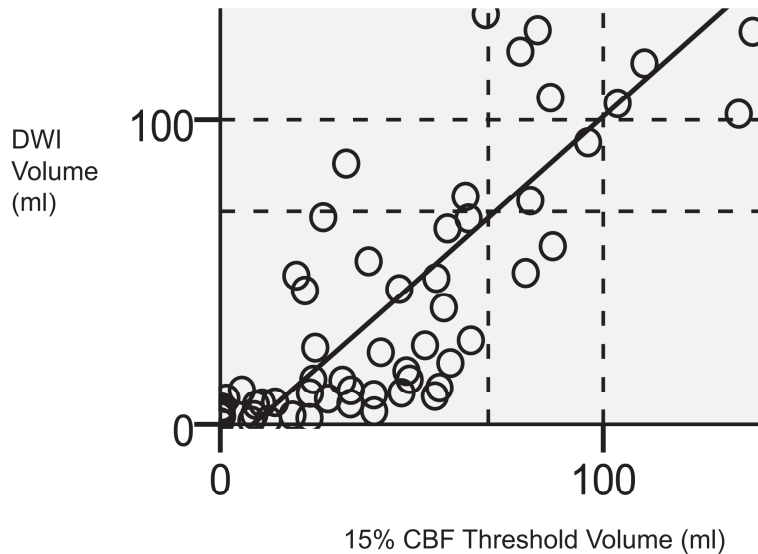


Figure A3

Figure A3. Comparison of DWI and CTP-derived cerebral blood flow estimates of core infarct volumes in the same patients with major anterior circulation occlusions. Analyses were performed on admission CTP and DWI of 62 stroke patients presenting with a large anterior circulation arterial occlusion on CTA. Infarct core was semi-automatically segmented on the admission DWI. A 15% thresholds was applied to the CBF map. Shown here are all patients with apparent core infarct volumes of less than ~150 ml on DWI or CBF. There was a high correlation between the 2 measurements ($R^2=0.87$, slope=1.11 for CBF; $p<0.001$). However, as illustrated here, there was a wide discordance between the DWI and CBF measurements in individual patients. From Souza, Lev, Franceschi, Hi, Gonzalez,

Schaefer. Thresholded CTP Maps Can Accurately Determine Infarct Core When DWI Is Unavailable, and Have Similar Specificity in Identifying Patients Unlikely to Benefit from Thrombolysis. Data presented at 2011 Radiological Society of North America Annual Meeting.

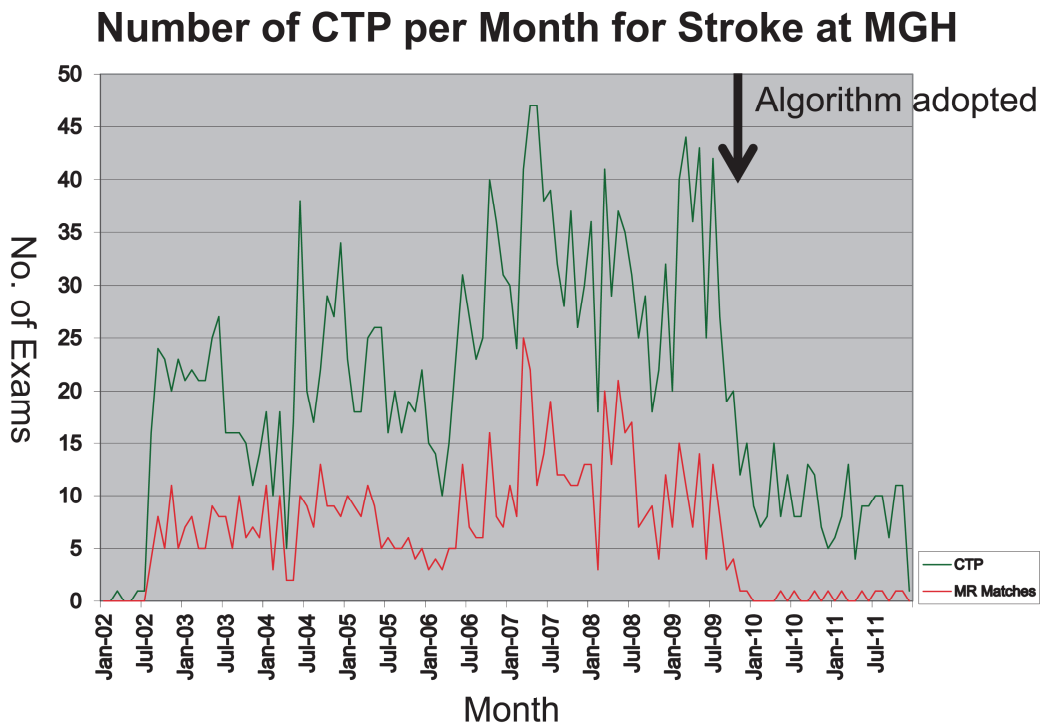


Figure A4

Figure A4. Monthly CT perfusion studies performed at MGH. The graph shows the number of CTP studies performed per month for stroke (green line) from July 2002 through December 2011. The red line shows the number of MRIs that were also performed on the same patients who had had CTP studies done. After we adopted this algorithm the number of CTPs dropped sharply (arrow).

Appendix Figure References

1. Powers WJ, Press GA, Grubb RL, Jr., et al. The effect of hemodynamically significant carotid artery disease on the hemodynamic status of the cerebral circulation. *Annals of Internal Medicine* 1987;**106**:27-34.
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4. Hakimelahi R, Yoo AJ, He J, et al. Rapid identification of a major diffusion/perfusion mismatch in distal internal carotid artery or middle cerebral artery ischemic stroke. *BMC Neurol* 2012;**12**:132.